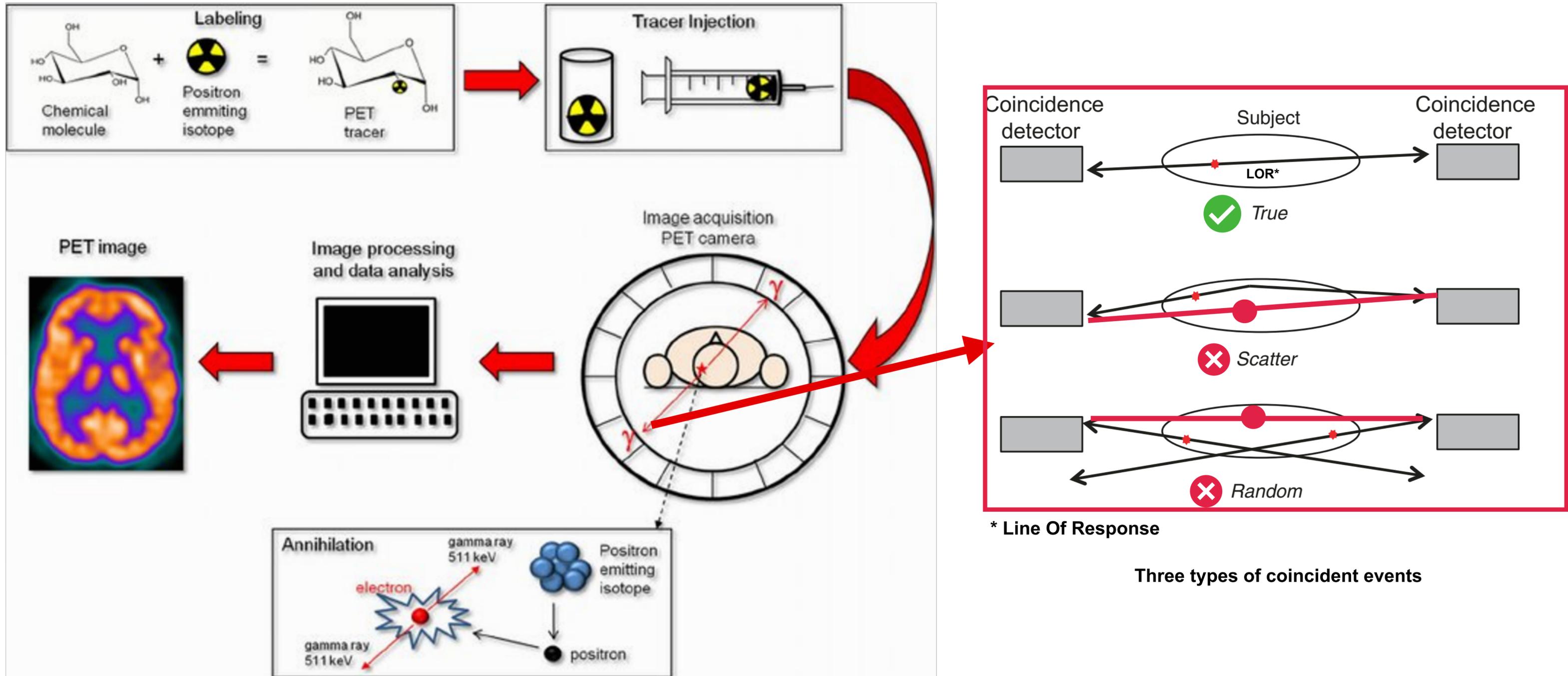




3D π scanner, an application in medical physics of the DarkSide collaboration

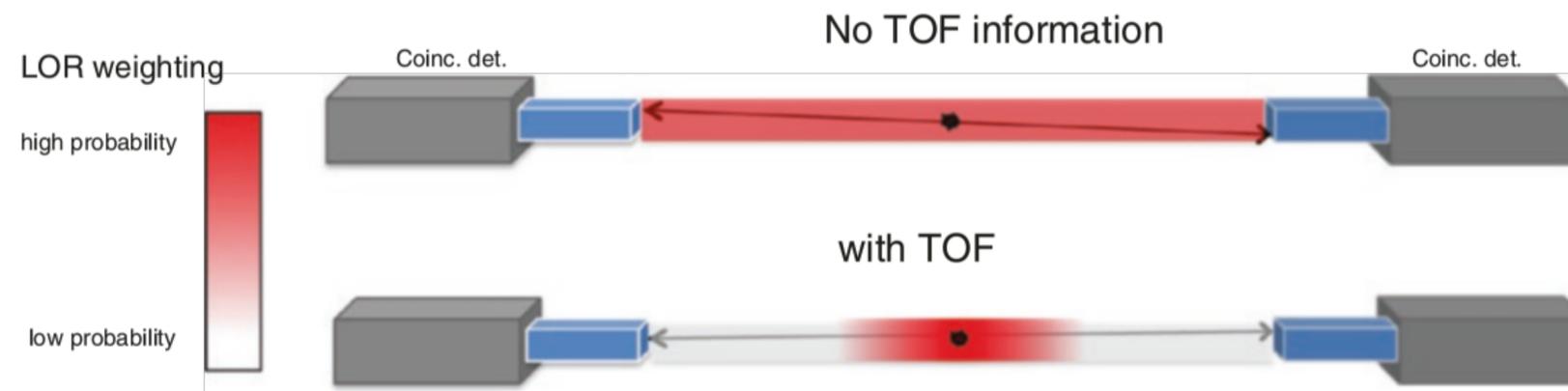
Azam Zabihi, ASTROCENT/CAMK-PAN, Warsaw, Poland (azabihi@camk.edu.pl)
On behalf of the 3D π TB-TOF-PET Collaboration

What is Positron Emission Tomography (PET)? How does it Work?



Credit: https://www.researchgate.net/publication/262189675_PET_imaging_in_multiple_sclerosis

Conventional PET vs. Time of Flight (TOF) PET

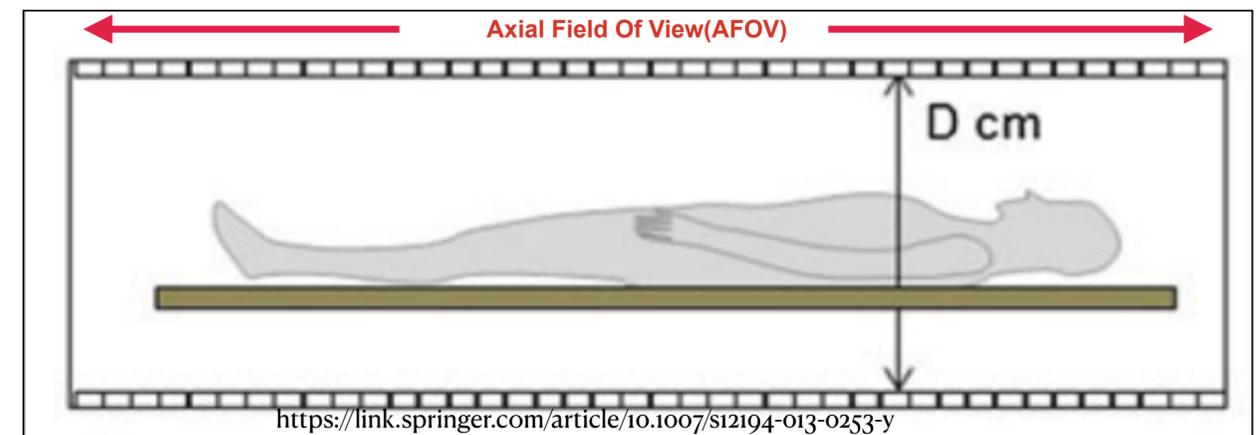
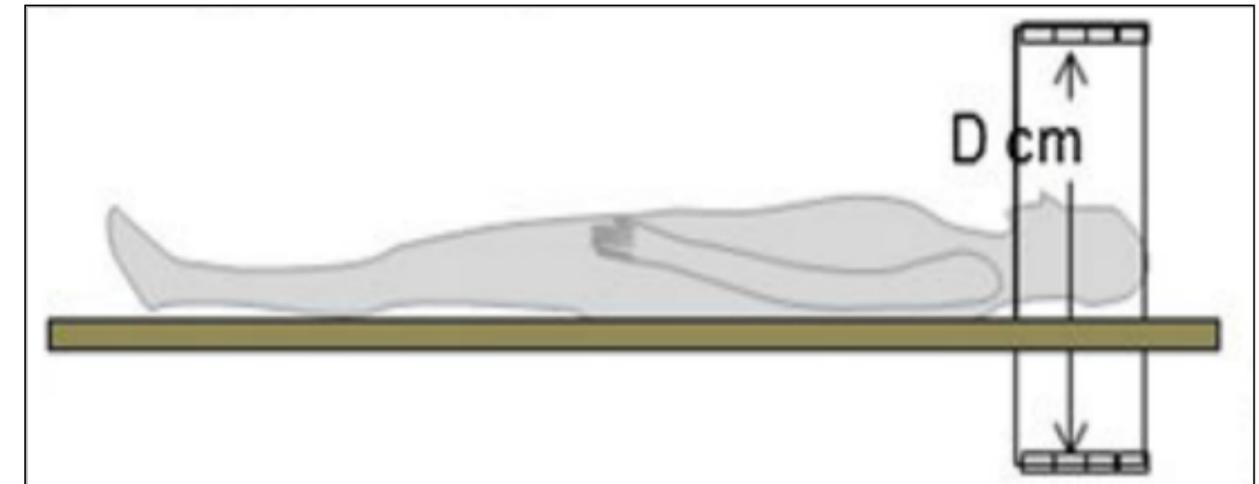


<https://link.springer.com/book/10.1007/978-3-319-40070-9>

✓ TOF-PET

- ◆ Limiting the event localization probability along the line of response (LOR)
- ◆ **Better locate the annihilation position** of the emitted positron

Routine PET vs. Total-Body PET (TB-PET)



<https://link.springer.com/article/10.1007/s12194-013-0253-y>

✓ Total body

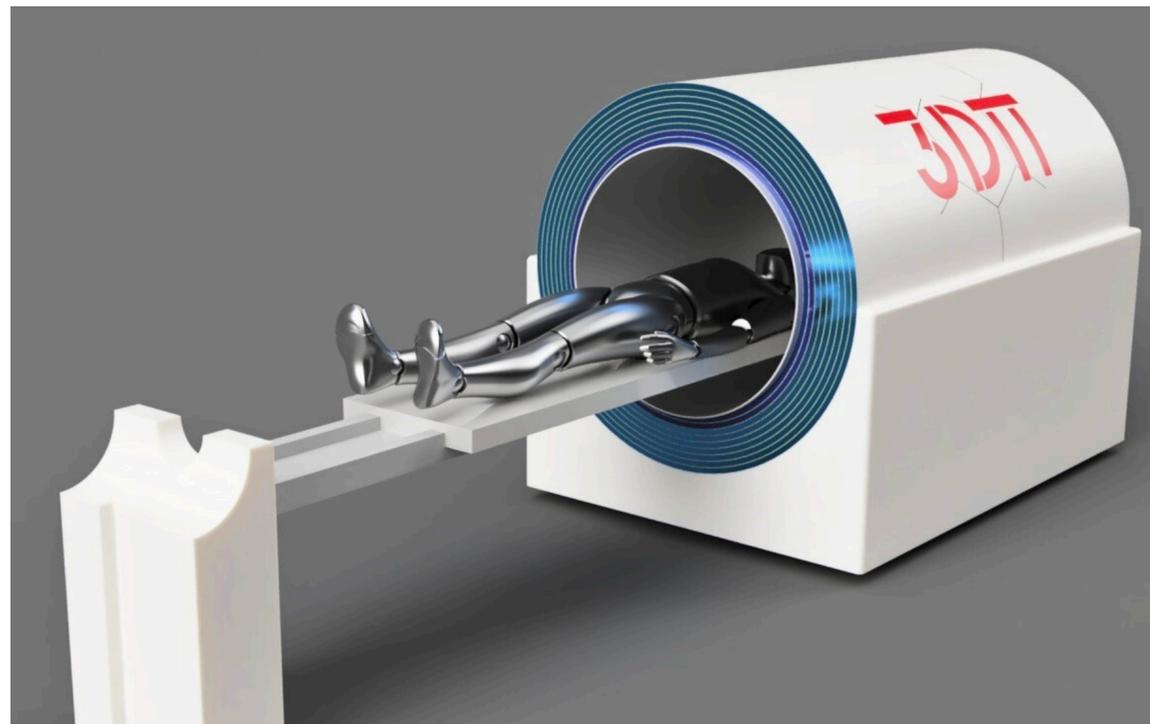
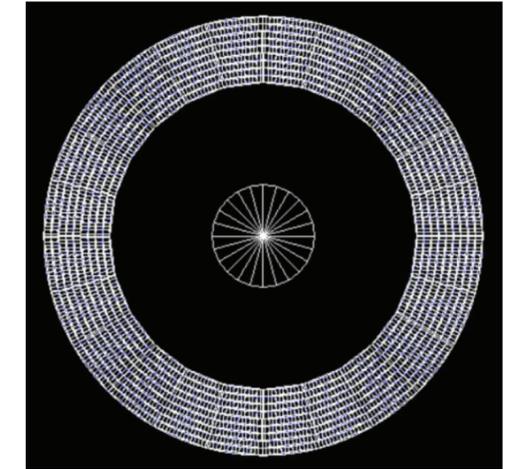
- ◆ Trace whole-body uptake images at the same time
- ◆ **Improve the sensitivity** dynamically
- ◆ **Reduce the scan time** dramatically

Our 3-Dimensional Positron Emission Tomography scanner (3DPi) Monte Carlo Simulation

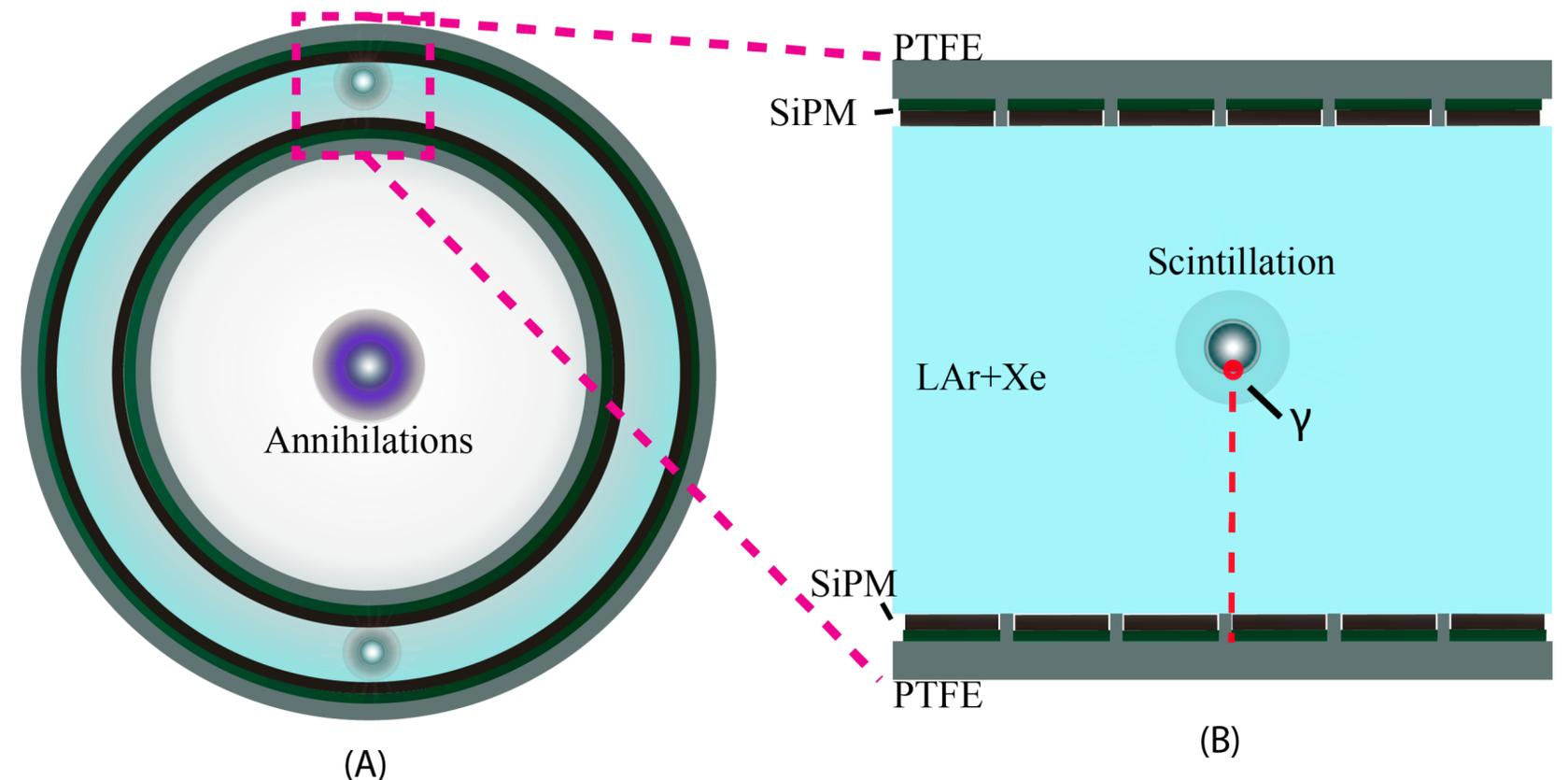
- ✦ Length: 2 m (Total Body)
- ✦ Inner radius: 45 cm
- ✦ Outer radius: 64 cm
- ✦ 9 annulus detection rings (Multiple layers)
- ✦ Each ring has Liquid Argon sandwiched Between two layers of SiPMs

- ✦ SiPM size: $10 \times 10 \text{ mm}^2$
- ✦ Number of SiPMs $\sim 10^6$ channels
- ✦ PTFE (Teflon) supporting structure

Geant4 Geometry Cross-section



Fusion 360 CAD model render of the 3DPi geometry



Single detection layer of the 3DPi detector with the LAr+Xe scintillation configuration.

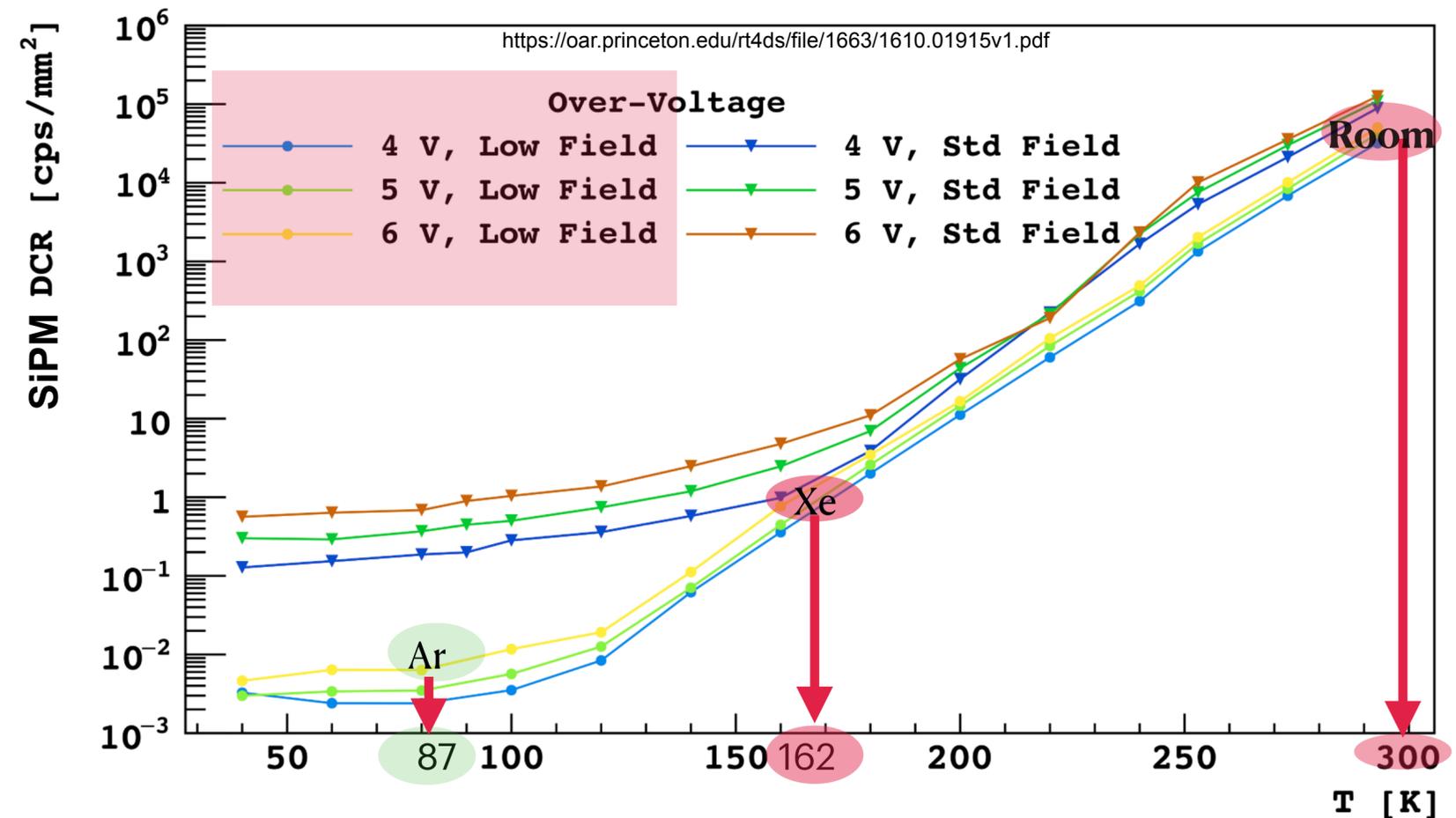
Each detection layer contains bottom and top layer of PTFE supporting material with an array of SiPMs.

Liquid Xenon vs. Liquid Argon

Credit: arXiv:1403.0525

Property	LAr	LXe	LAr+LX
Fast decay time (ns)	7	4.3	~6
Slow decay time (ns)	1600	22	~100
Light yield (Photons/keV)	40	42	41
Wavelength (nm)	128	175	~175
Density (g/cm ³)	1.40	2.94	~1.40
Temperature (K)	87	162	87
Cost (US\$/kg)	~2	~2000	~2

SiPM Dark Count Rate (DCR) vs. Temperature



Reduction in the dark count rate improves the timing capability of the devices

Combine the advantages of both ==> Xenon-doped Liquid Argon (Xe concentration ~100 ppm)

- *Scintillation light at a wavelength of 175 nm (as a WLS)
- *Operation at temperatures close to the argon boiling point, so don't need cooling down and have lower DCR
- *Shorter slow decay time than the pure liquid argon

National Electrical Manufacturers Association, NEMA NU 2-2018

A guide to characterize PET performance

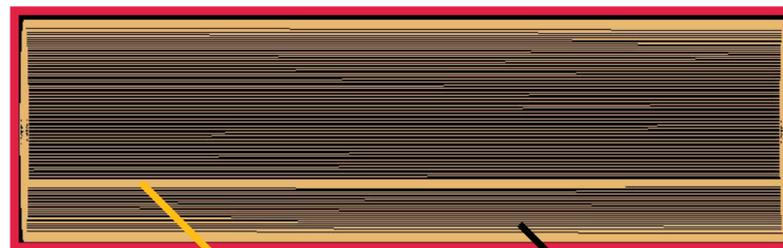
Noise Equivalent Count Rate (NECR)

$$\frac{T^2}{T+S+R}$$

T: True coincidences count rate

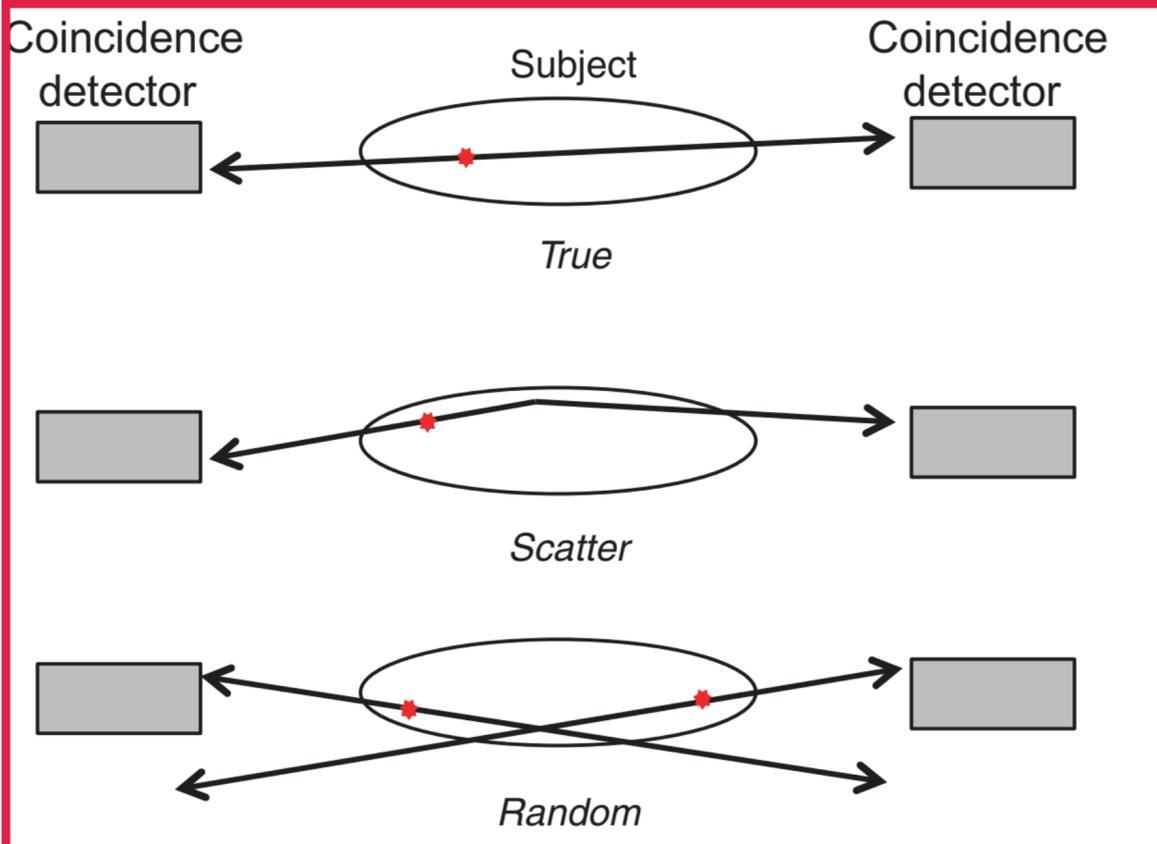
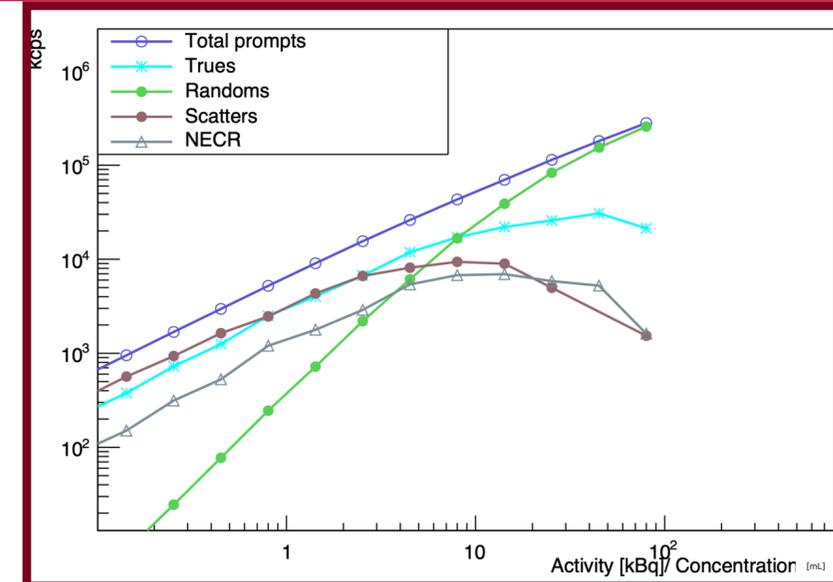
S: Scattered coincidences count rate

R: Random (accidental) coincidences count rate



Line Source

Test Phantom



Three types of coincident events

Scanner

Peak NECR

Activity concentration at peak

Scatter Fraction at peak

Our PET (MC) (Preliminary)

~10⁴ kcps

7.7 kBq/mL

35.2%

EXPLORER TB-PET/CT (Actual)

~10³ kcps

17.3 kBq/mL

37.4%

GE SIGNA PET/CT (Actual)

218 kcps

17.8 kB/mL

43.6%

CareMainBrain PET (Actual)

49 kcps

~14 kB/mL

48%

Higher NECR at lower activity decay rate means extremely reduction radiopharmaceutical dose

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A guide to characterize PET performance

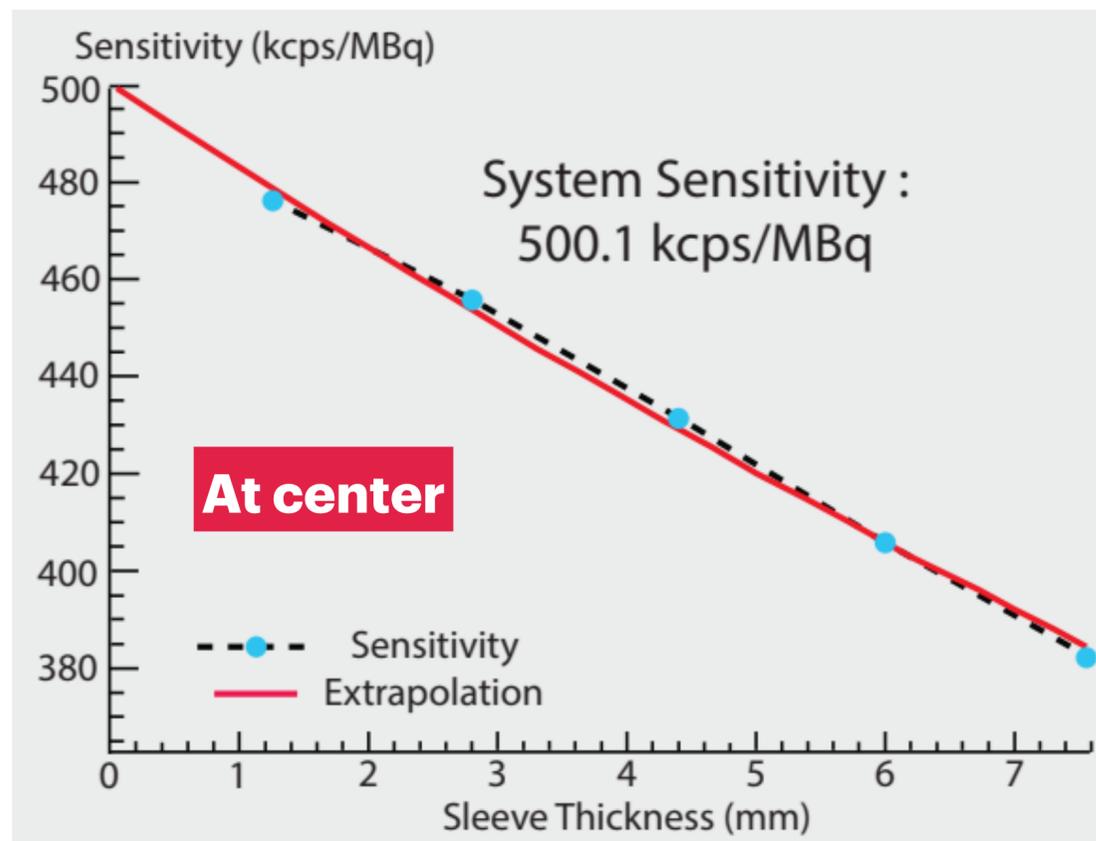
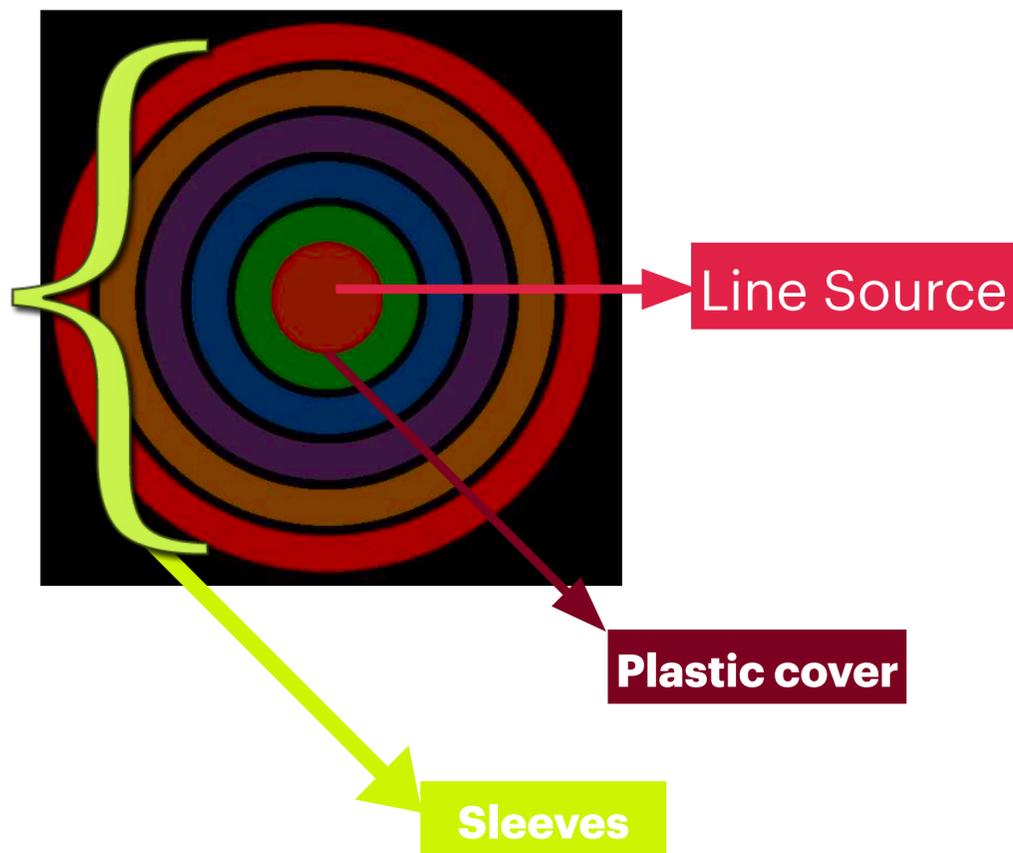
The sensitivity test measures the counts per second that the scanner measures for every unit of activity present in a source.

$$S_{\text{tot}} = \frac{R_{\text{CORR},0}}{A_{\text{cal}}}$$

S_{tot} : System Sensitivity

$R_{\text{CORR},0}$: The true coincidences count rate with no attenuation

A_{cal} : Line source radioactivity



System Sensitivity at center

(Preliminary)

Our Total-Body TOF-PET
500 kcps/MBq

EXPLORER Total-Body PET/CT
147 kcps/MBq

CareMainBrain PET
13.82 kcps/MBq

At low decay activity

Summary

3D π PET Scanner

- ❖ LAr+Xe as scintillation material, operates at temperatures close to the argon boiling point, So it reduces SiPM DCR.
- ❖ LAr+Xe as scintillation material, operates as WLS, and shifts optical photon wavelength 128 nm (LAr) to 178 nm (Xe).
- ❖ LAr + Xe + SiPMs allows for fast scintillation and better timing and spatial resolution.
- ❖ Higher NECR at lower activity decay rate and higher sensitivity means extremely reduction of the whole-body imaging duration or the lessen of the radiopharmaceutical dose

Ongoing activities

- ◆ Setup at INFN Cagliari, to test coincidence time resolution in the liquid argon-xenon mixture (Funding:300k€)
- ◆ Setup at Princeton to test stability of the Xe-doped LAr
- ◆ Agreement with Fondazione Bruno Kessler (FBK) to test their SiPM sensitive to Xe scintillation with ASIC
- ◆ Testing of the ALCOR chip (ASIC) from INFN Torino at cryogenic temperature

Future work on MC simulation

- ✱ Optimizing SiPM size
- ✱ Optimizing layer geometry
- ✱ New reconstruction algorithms

Current Collaboration

- ✱ Princeton University
- ✱ ASTROCENT
- ✱ University of Houston
- ✱ Lawrence Berkeley National Laboratory
- ✱ University of Cagliari
- ✱ INFN
- ✱ APC, University of Paris, CNRS
- ✱ Gran Sasso Science Institute



Thanks for your attention